

# Potential conflicts of interest and Safe Harbor Statement

**Speaker's name: Mark Landy**

- I have the following potential conflicts of interest to report:
  - President and CEO MIV Therapeutics
  - Stockholder of MIV Therapeutics

Except for the historical information contained herein, the matters discussed in this presentation are forward-looking statements. Such statements are indicated by words or phrases such as "believe," "will," "breakthrough," "significant," "indicated," "feel," "revolutionary," "should," "ideal," "extremely" and "excited." These statements are made under "Safe Harbor" provisions of the Private Securities Litigation Reform Act of 1995. Actual results may differ materially from those described in forward-looking statements and are subject to risks and uncertainties. See the Company's filings with the Securities and Exchange Commission including, without limitation, the Company's recent Form 10-K and Form 10-Qs, which identify specific factors that may cause actual results or events to differ materially from those described in the forward-looking statements



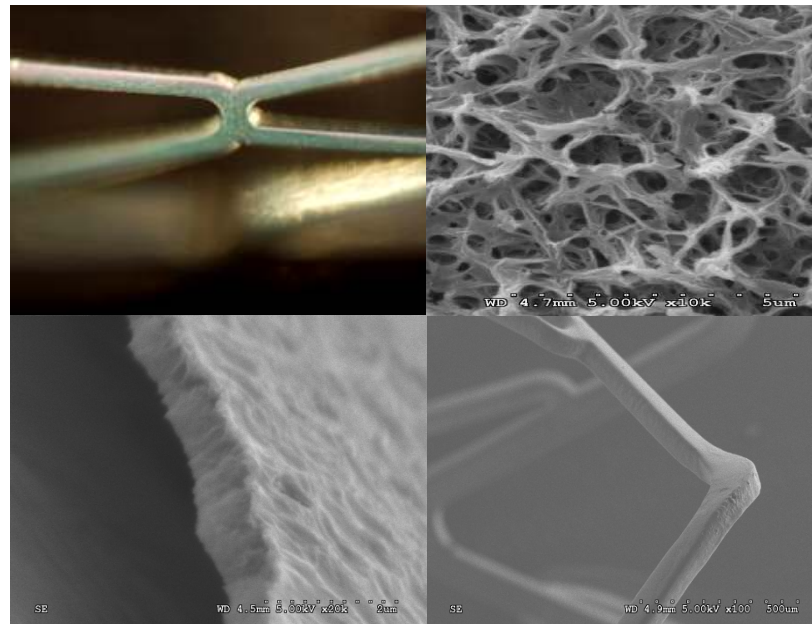
# A Novel Polymer Free Hydroxyapatite Based Drug Delivery Stent

**Mark Landy, President and CEO**

## MIV Polymer-Free DES Combine A Novel NanoPorous HAp Surface Modification With Lipid-Based Drug Delivery Technologies And Release Drug In Capsules

The HAp lattice provides the structural rigidity required to allow the use of lipid-based drug delivery technologies which deliver the drug in capsules

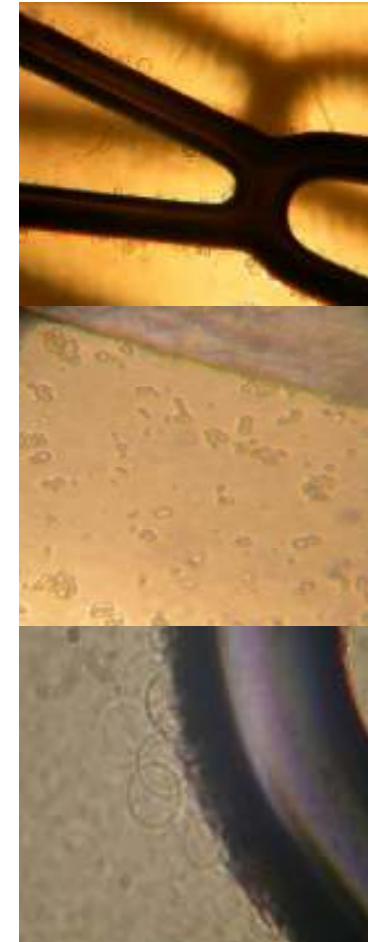
Drug mixtures are loaded into the hydroxyapatite pores to form an ultra-flexible drug delivery coating that is 0.6 microns thin and extremely durable



MIV DES do not require significantly more time and resources to manufacture than current DES and have current DES-like margins

# Drug Encapsulation Positively Impacts Safety And Efficacy

- I. Improves the uptake of drug by local cells
- II. Can targets the delivery of drug against specific cells
- III. Houses drug in a capsule protecting surrounding tissue
- IV. Can amplify or suppress the different mechanisms of action of a single drug at different time points in the elution curve
- V. Provides a hydrophobic matrix to deliver hydrophilic drugs preventing early washout



# Introducing A DES With The Safety Profile of a Bare Metal Stent

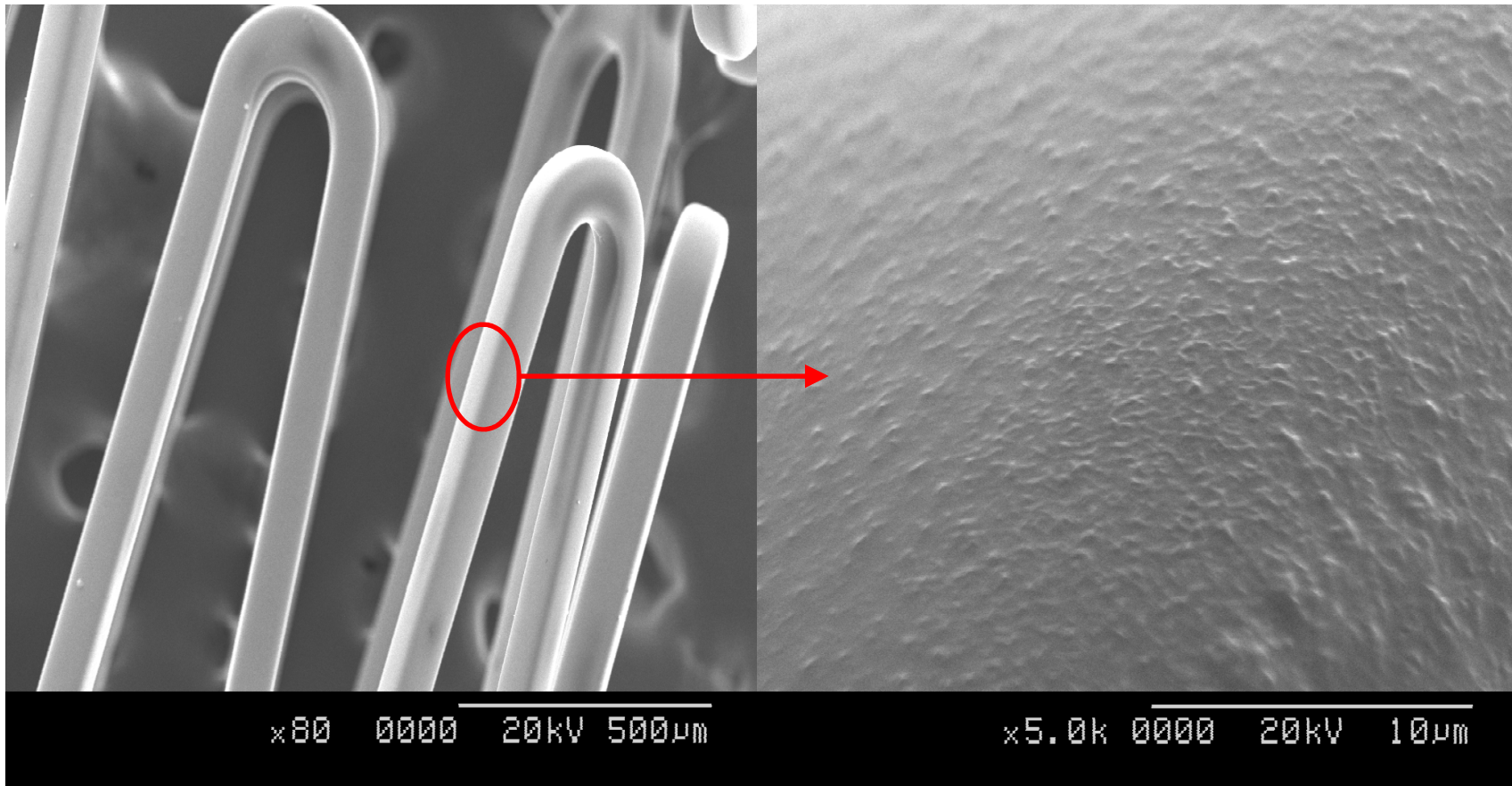
**VESTASync<sup>TM</sup>**  
Sirolimus Eluting Coronary Stent System

# A Massive Technology Advantage

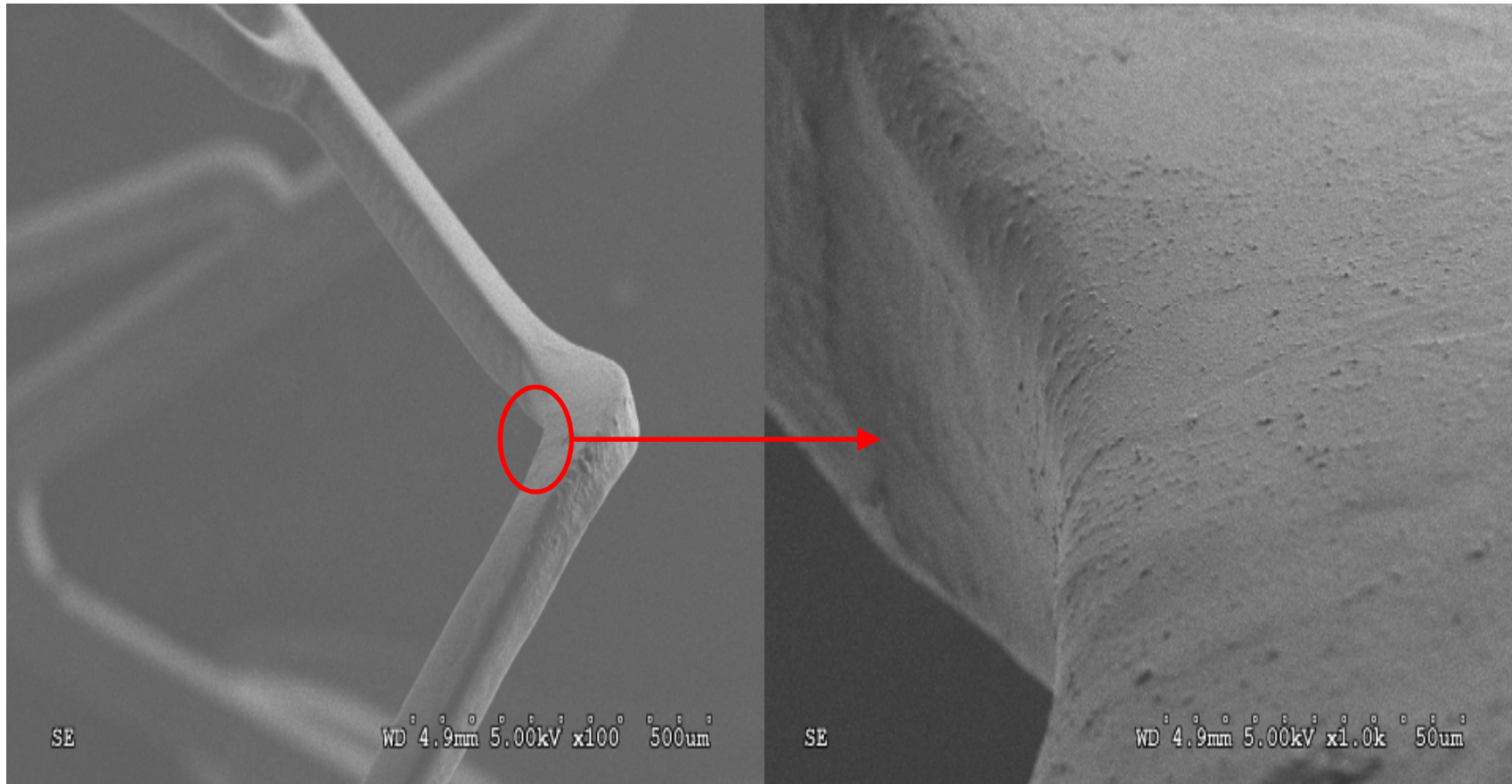
Thin Struts  
Polymer-Free  
Low Drug Dose  
Complete Healing  
Competitive Efficacy  
Excellent Deliverability  
Short Anti-Platelet Therapy

A Drug Eluting Stent With The Safety Profile  
And Deliverability of A Bare Metal Stent

# Uniform Surface Finish



# Superb Coating Integrity





# 25% Thinner Struts Than Xience™ V 60% Less Drug Than Cypher®

Minimizing Strut and Polymer Thickness to reduce Injury and aid re-endothelialization

CYPHER®	TAXUS® Liberté	ENDEAVOR™	XIENCE™ V
<b>Strut Thickness:</b> <b>140 µm</b>	<b>Strut Thickness:</b> <b>132 µm</b>	<b>Strut Thickness:</b> <b>91 µm</b>	<b>Strut Thickness:</b> <b>81 µm</b>
<b>Polymer Thickness:</b> <b>13.7 µm</b>	<b>Polymer Thickness:</b> <b>16.4 µm</b>	<b>Polymer Thickness:</b> <b>4.8 µm</b>	<b>Polymer Thickness:</b> <b>7.8 µm</b>
<b>PEVA+PBMA</b>	<b>SIBBS:</b>	<b>PC</b>	<b>Fluoropolymer</b>
<b>Sirolimus</b>	<b>Paclitaxol</b>	<b>ABT 578</b>	<b>Everolimus</b>
<b>154 µm</b>	<b>148 µm</b>	<b>96 µm</b>	<b>89 µm</b>

Photos & data on File at Abbott Vascular

**VESTAsync™**

<u>Strut Thickness</u>	65 µm
<u>Coating Thickness</u>	0.6 µm
<u>Coating Material</u>	HAp + Lipid
<u>Drug Dose</u>	57 ug Sirolimus *
<u>DES Strut Thickness</u>	66 µm
<u>Source</u>	MIV

**AVPath**

\* VESTAsync™: 57ug/19mm stent or 3.0ug/mm Vs. Cypher: 140ug/19mm stent or 7.4 ug/mm

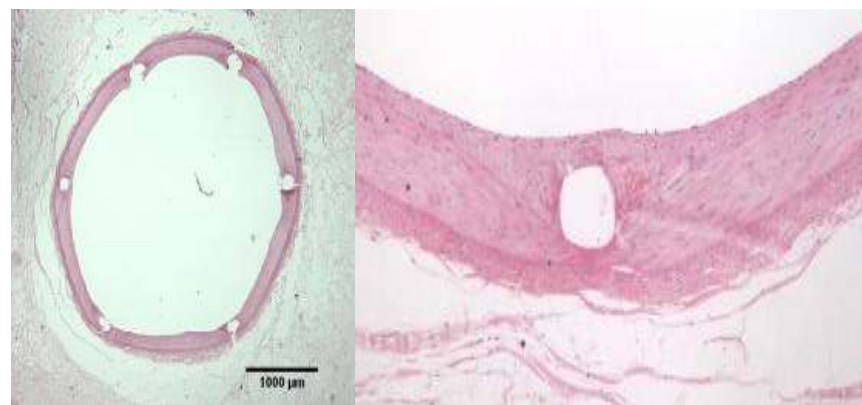
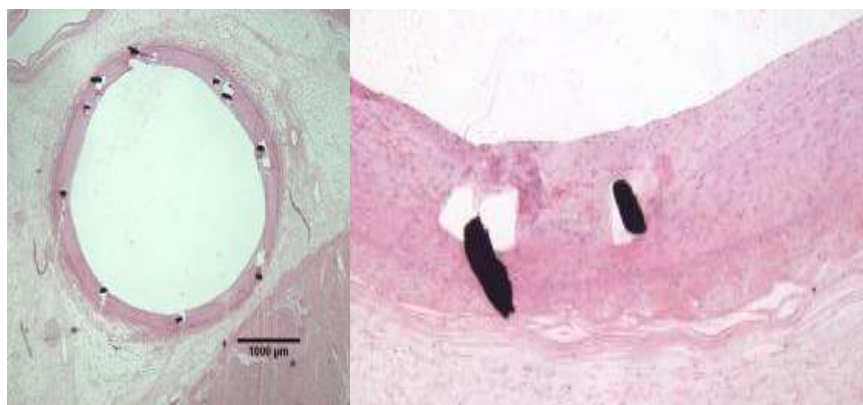
# Excellent Morphometric Data

## VESTAsync™

Injury Score	S/A Ratio	NI Stent (um)
0.3 ± 0.5	1.1 ± 0.1	236 ± 93

## Cypher

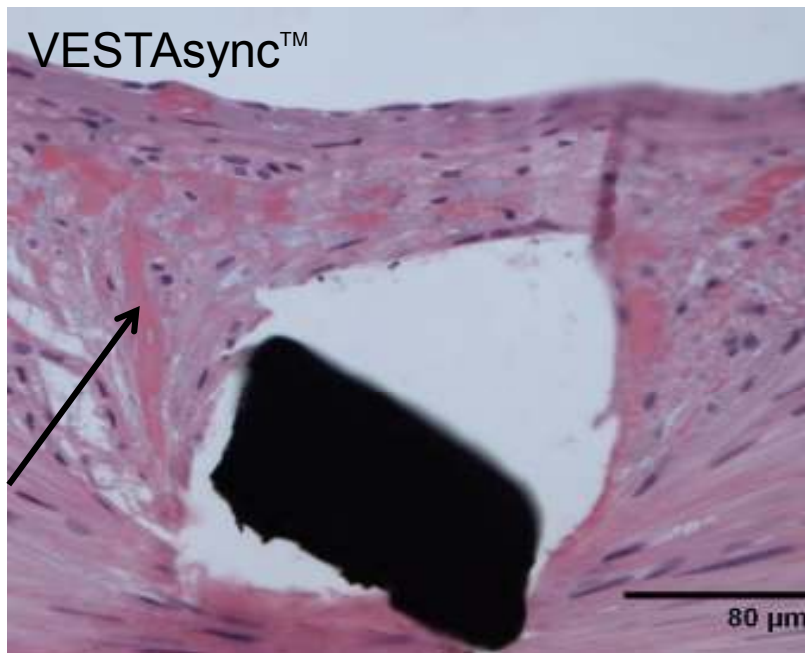
Injury Score	S/A Ratio	NI Stent (um)
0.4 ± 0.5	1.1 ± 0.1	282 ± 102



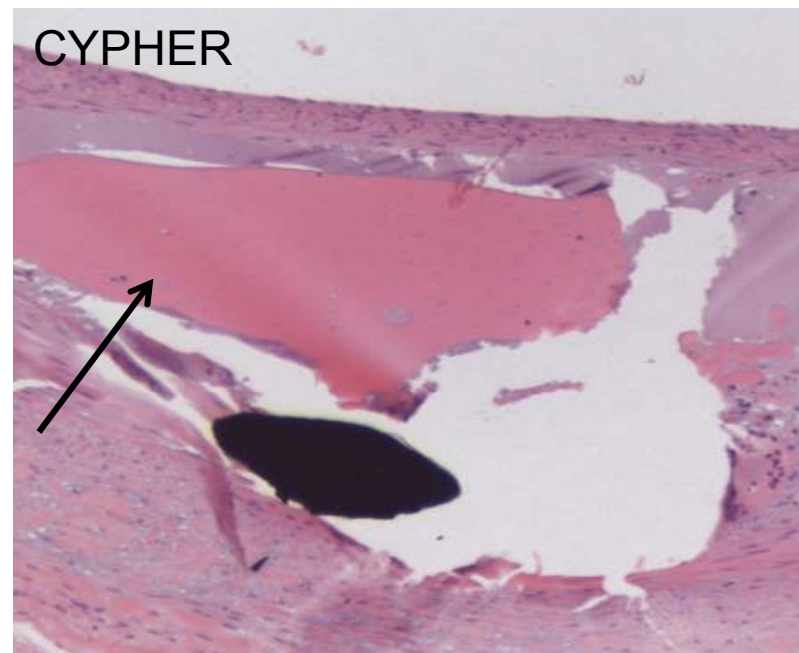
At 28 days the VESTASYNC showed good neointimal healing with complete strut coverage and little inflammation versus incomplete healing with uncovered struts and high levels of inflammation for the Cypher

Source: van der Giessen EUROPCR 2007

# 75% Less Fibrinoid Material



Minimal Fibrinoid (.03%)

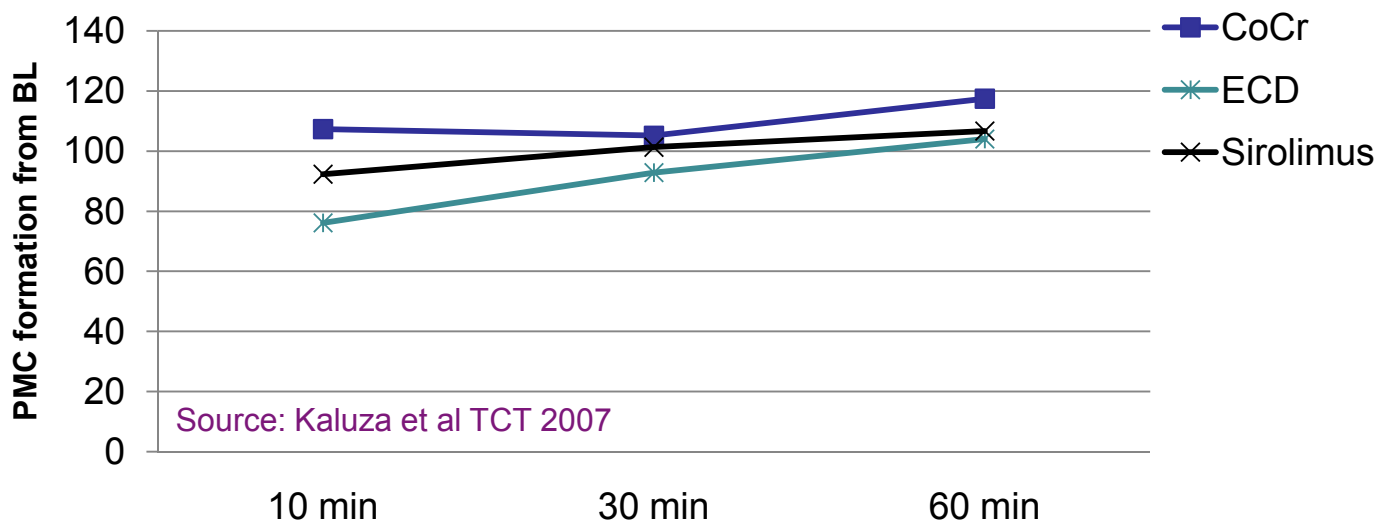
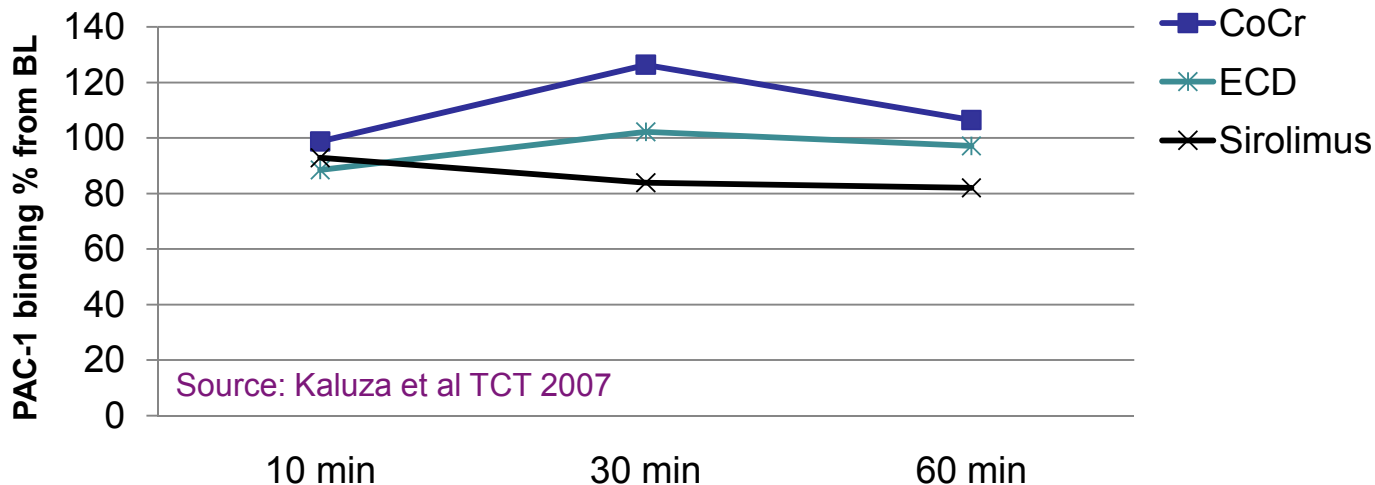


Excessive Fibrinoid (.12%)

At 28 Days the VESTASYNC exhibited a statistically significant ( $P=0.004$ ) lower amount of fibrinoid material, a marker for delayed healing

Source: van der Giessen et al EUROPCR 2007

# BMS-Like Platelet Activation



# Positive VESTASYNC-I FIM Study

Single De novo lesions in native coronary arteries of 15 patients

RVD: 3.0 - 3.5 mm

Lesion length:  $\leq 14$ mm

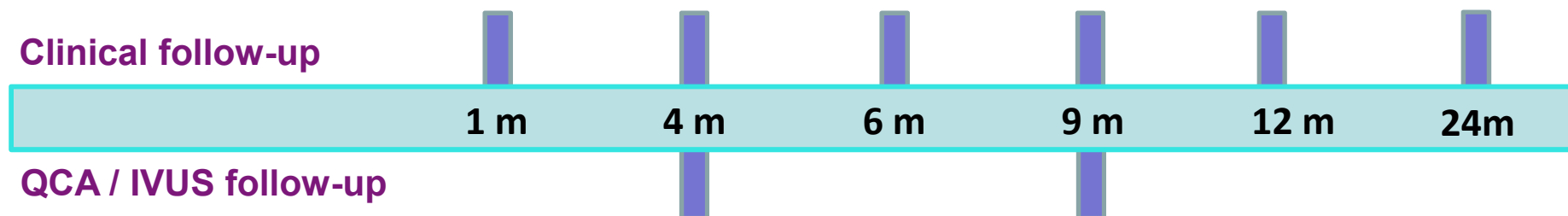
Stent diameters : 3.0 and 3.5mm

Stent length: 19mm

Pre dilatations mandatory

**PI: Alexandre Abizaid MD, PhD**

Clinical follow-up



QCA / IVUS follow-up

Primary Endpoint

In-stent lumen loss at 4-month follow-up by QCA

Secondary Endpoints

MACE up to 24 months

Acute success

TLR and TVR up to 24 months

In-stent and in-segment NIH volume at 4 months

**Single Center:**

Brazil (Instituto Dante Pazzanese)

**Dual anti-platelet therapy for 5 months**

The VESTASYNC-I FIM study met its primary safety and efficacy endpoints. Matched QCA analysis of 12 pts at 4 and 9 months showed no increase in LLL (P=0.9)

Variable (n=15)	In-Stent 4-Month	In-Segment 4-Month
MLD, mm	2.34 ± 0.36	2.02 ± 0.37
% Diameter stenosis	13.8 ± 7.0	23.6 ± 8.8
Late lumen loss, mm	<b>0.30 ± 0.25</b>	<b>0.16 ± 0.29</b>
Restenosis*, % (n)	0.0 (0)	0.0 (0)

Variable (n=12**)	In-Stent 4-Month	In-Segment 4-Month	In-Stent 9-Month	In-Segment 9-Month
MLD, mm	2.33 ± 0.34	2.05 ± 0.37	2.27 ± 0.33	2.02 ± 0.29
% Diameter stenosis	±	±	15.9 ± 8.2	23.6 ± 9.5
Late lumen loss, mm	<b>0.31 ± 0.26</b>	<b>0.17 ± 0.32</b>	<b>0.37 ± 0.24</b>	<b>0.20 ± 0.31</b>
Restenosis*, % (n)	0.0 (0)	0.0 (0)	0.0 (0)	0.0 (0)

\* Defined as diameter stenosis ≥ 50% at angiographic follow up

\*\* 3 patients refused 9-month follow up

Source: Abizaid et al ACC 2008

## Matched IVUS analysis of 11 patients at 4 and 9 months showed no increase in NIH volume or percentage obstruction (P=0.8)

Variable	Baseline n=14*	4-Month n=14*
Vessel Volume (mm <sup>3</sup> )	276.7 ± 117.1	276.6 ± 84.8
Stent Volume (mm <sup>3</sup> )	145.7 ± 14	142 ± 0.5
Lumen Volume (mm <sup>3</sup> )	145.8 ± 47.5	138.8 ± 33.5
NIH Volume (mm <sup>3</sup> )	N/A	<b>3.9 ± 3.3</b>
Mallapposition Volume (mm <sup>3</sup> )	0.15 ± 0.5	0.09 ± 0.3
% Stent Obstruction	N/A	<b>2.6 ± 2.22</b>
Variable	4-Month N= 11 P*	9-Month N= 11 P*
Vessel Volume (mm <sup>3</sup> )	286.9 ± 87.4	296.8 ± 85.6
Stent Volume (mm <sup>3</sup> )	140.5 ± 36.7	143.1 ± 41.4
Lumen Volume (mm <sup>3</sup> )	136.3 ± 34.2	136.8 ± 38.2
NIH Volume (mm <sup>3</sup> )**	<b>4.3 ± 3.5</b>	<b>6.1 ± 4.9</b>
Mallapposition Volume (mm <sup>3</sup> )	0.14 ± 0.34	0.13 ± 0.36
% Stent Obstruction**	<b>2.8 ± 2.2</b>	<b>3.8 ± 2.3</b>

IVUS consol hard drive malfunction prevented retrieval of data for patient #14 \*\* 3 Patients refused 9-month follow up

Source: Abizaid et al ACC 2008

# VESTASYNC-1 FIM Nine-Month MACE

Variable	Patients (n=15)
<b>In-hospital</b>	
<i>Death, n(%)</i>	0
<i>MI, n(%)</i>	0
<i>TLR, n(%)</i>	0
<i>Stent thrombosis, n(%)</i>	0
<b>4-month follow-up</b>	
<i>Death, n(%)</i>	0
<i>MI, n(%)</i>	0
<i>TLR, n(%)</i>	0
<i>TVR, n (%)</i>	0
<i>Stent thrombosis, n(%)</i>	0
<b>9-month follow-up</b>	
<i>Death, n(%)</i>	0
<i>MI, n(%)</i>	0
<i>TLR, n(%)</i>	0
<i>TVR, n (%)</i>	0
<i>Stent thrombosis, n(%)</i>	0

Source: Abizaid et al ACC 2008



# Summary

- I. Differentiated approach and a strong patent position
- II. Strong proof of concept in animals and humans
- III. Opportunity to revolutionize DES therapy and significantly expand the stent market and usage

